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## Nanostructure of carious tooth enamel lesion

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### ABSTRACT

Carious lesions exhibit a complex structural organization composed of zones of higher and lower mineralization, formed by successive periods of cyclic de- and re-mineralization. A thorough understanding of the lesion morphology is necessary for the development of suitable treatments aiming to repair rather than replace the damaged tissue. This detailed understanding includes the entire lesion down to individual crystallites and nanopores within the natural organization of the crown. A moderate lesion, with surface loss and reaching dentin, and a very early lesion were studied. Scanning small-angle X-ray scattering (SAXS) with a pixel size of  $20 \times 20 \mu\text{m}^2$  was used to characterize these lesions, allowing for the identification of distinct zones with varied absorption and scattering behavior, indicative of varied porosity and pore morphology. Despite these differences, the overall orientation and anisotropy of the SAXS signal was unaltered throughout both lesions, indicating that an anisotropic scaffold is still present in the lesion. The finding that crystallite orientation is preserved throughout the lesions facilitates the identification of preventive re-mineralizing strategies with the potential to recreate the original nanostructure.

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### 1. Introduction

Caries is the most prevalent of all chronic childhood diseases and the leading cause of tooth loss among young adults in many societies [1–3]. Caries causes considerable suffering, loss of function and the need for costly restorative, endodontic and prosthetic interventions. However, behavioral, dietary, preventive and interventional actions can re-mineralize early lesions [4–6]. Improved knowledge of the carious process, de- and re-mineralization, at the component or nano-structural level could facilitate improved preventive and therapeutic approaches for early lesions and allow moderate lesions to be addressed.

Caries is a chronic hard tissue infection [7]. Smooth surface caries has been studied extensively, not just because of its epidemiological importance, but also because a relatively simple geometry facilitates studies and experimental modeling. Lesions have been studied in many ways, including macroscopic examination, hard tissue histology, light microscopy, scanning and transmitted electron microscopy, microradiography, micro and nano indentation, histochemical, microbiological and chemical analyses, and X-ray imaging techniques [8–19]. These methods have provided a wealth of information and allowed various zones to be identified. Electron microscopy has been used to observe microstructural changes such as clefts or channels in incipient lesions and to identify de- and

re-mineralization-induced changes to individual crystallites, but generally only after they have been removed from their original spatial organizational positions and associations with their neighbors. Detailed understanding, or mapping, of the entire lesion at the level of individual crystallites and porosities remains elusive.

Differences in optical birefringence caused by the submicroscopic pores produced during de-mineralization have been used to divide the smooth surface lesion into four zones [15,20,21]: first, an outer surface layer of intact relatively unaffected enamel, displaying negative birefringence to polarized light, radio-opacity, with some focal holes and  $\sim 10\%$  mineral loss; second, the body of the lesion, with positive birefringence to polarized light, radiolucency and substantial mineral loss of  $\sim 24\%$ ; third, the dark zone, with positive birefringence to polarized light, radio-opacity and  $\sim 6\%$  of mineral loss; finally, the translucent zone with negative birefringence to polarized light, radio-opacity and only  $\sim 1\%$  mineral loss. However, this classification does not describe changes in crystallite structure or organization. Furthermore, smaller and deeper pores are not discerned by birefringence [22].

Small-angle X-ray scattering (SAXS) is capable of delivering structural information about macromolecules or crystallites and of repeat distances in partially ordered systems as small as a few nanometers in size and up to several hundred nanometers [23–33]. This range is well suited to studying hydroxyapatite crystallite and collagen periodicities, the primary components of tooth structure. The combination of SAXS with real-space scanning [34] allows for the investigation of a tooth's nano-structural

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components over extended areas through the acquisition of thousands scattering patterns [23,29–31,35,36]. Two-dimensional (2-D) maps with raster-scan step sizes as small as  $0.1 \times 0.1 \text{ mm}^2$  have been made [31]. Because an early carious lesion may be only 0.1–0.2 mm in total thickness, and because features within a moderate lesion may be <0.1 mm thick, increased point density is needed to study the four zones generally used to describe smooth surface caries. Scanning SAXS with raster-scan step sizes of  $20 \times 20 \text{ }\mu\text{m}^2$  is applied. This high point density allows the identification and comparison of morphological differences within and among carious zones with respect to structural organization: orientation and degree of anisotropy of the nanometer-size components.

## 2. Materials and methods

### 2.1. Carious specimens

Two representative naturally occurring smooth surface carious lesions, moderate and early, obtained from two third molars extracted for clinical reasons, were studied. All procedures were conducted in accordance with the Declaration of Helsinki and according to the ethical guidelines of the Canton of Basel, Switzerland. Teeth were extracted for clinical reasons unrelated to the study. Written consent by the patients concerning use of the extracted teeth is given in the patient entry form of the dental school. The consent is not study specific. Teeth are anonymized. Backtracking of patient identity is impossible and not desired. The moderate lesion (specimen H) had slight surface loss and appeared to barely reach beyond the dentino-enamel junction (DEJ). The early lesion (specimen V) was smaller and incipient, without surface breakdown, and limited to the outer third of the enamel. The tooth slices were cut using a diamond band saw (Exakt Apparatebau GmbH, Norderstedt, Germany). A  $200 \text{ }\mu\text{m}$  thin slice was cut in a transverse direction through the moderate lesion, while a  $200 \text{ }\mu\text{m}$  thin slice was obtained through the early lesion in the buccal-lingual direction (see Fig. 1). The slices were stored in phosphate buffered saline before and during measurements.

### 2.2. Conventional micro computed tomography

Micro computed tomography ( $\mu\text{CT}$ ) data sets of the entire teeth were acquired with a Skyscan 1174<sup>TM</sup> tabletop scanner (Bruker, Belgium), and 900 projections with a pixel size of  $35.6 \text{ }\mu\text{m}$  were acquired over  $360^\circ$ . The acceleration voltage was set to 50 kV and the beam current to  $800 \text{ }\mu\text{A}$ . The data were reconstructed using a modified Feldkamp algorithm (NRecon, Bruker, Belgium).

### 2.3. Synchrotron radiation-based $\mu\text{CT}$

Synchrotron radiation-based  $\mu\text{CT}$  (SR $\mu\text{CT}$ ) measurements were performed at the W2 beamline at HASYLAB (DESY, Hamburg, Germany) operated by the HZG research center [37]. For specimen V, the photon energy was set to 45 keV, and 1440 equiangular projections with a pixel size of  $4.6 \text{ }\mu\text{m}$  were acquired over  $360^\circ$ . The rotation axis was chosen asymmetrical to the incoming X-ray beam to allow for a larger field of view [38]. The data were reconstructed using a filtered backprojection algorithm. Specimen H was measured at a photon energy of 30 keV. The pixel size of the projections corresponded to  $3.2 \text{ }\mu\text{m}$ , and 900 projections were acquired over  $180^\circ$ .

### 2.4. SAXS data acquisition

Scanning SAXS measurements were performed at the cSAXS beamline [39] of the Swiss Light Source (Paul Scherrer Institute, Villigen, Switzerland). The specimens were stored in polyimide sa-

chets and placed on an aluminum holder. Scattering patterns were acquired in a raster scan fashion in the  $x$ - and  $y$ -directions perpendicular to the beam. For specimen V, the points at which SAXS data was acquired were  $50 \text{ }\mu\text{m}$  apart in both  $x$ - and  $y$ -directions, while for specimen H, a raster scan step size of  $20 \text{ }\mu\text{m}$  was chosen. The photon energy was set to 18.6 keV. The scanning in the horizontal, i.e.,  $x$ -, direction was performed with the detector recording a series of SAXS data, while the specimens moved at a velocity of 1.786 and  $0.714 \text{ mm s}^{-1}$ , respectively. The X-ray beam was focused to  $25 \text{ }\mu\text{m} \times 8 \text{ }\mu\text{m}$  full width at half-maximum (FWHM) spot size at the specimen position. In the first scan, the X-ray transmission of the specimens at each scanning position was recorded with no beam stop and an attenuated beam with 8 ms exposure time. In the second scan, the scattering patterns were recorded with two modules of the PILATUS 2 M detector [40] with 20 ms exposure time and 8 ms readout time. For specimen V, 32,000 frames were acquired, and for specimen H, 82,000 frames. The direct beam was covered with a beam stop 3 mm in diameter. The transmission data were used to correct the SAXS signal for specimen absorption. The specimen-detector distance of 7140 mm was determined with the first-order diffraction ring of a silver-behenate powder. To minimize air scattering, an evacuated flight tube was placed between specimen and detector.

### 2.5. SAXS data treatment

Each scattering pattern is divided into 16 azimuthal sectors, and the intensity is azimuthally integrated at each radial position, yielding, for each scattering pattern, intensities for the 16 segments as a function of  $q$ . The intensity in each segment for a chosen radial range, plotted against the segment angular position  $\phi$ , is approximated with a cosine by means of fast Fourier transform:

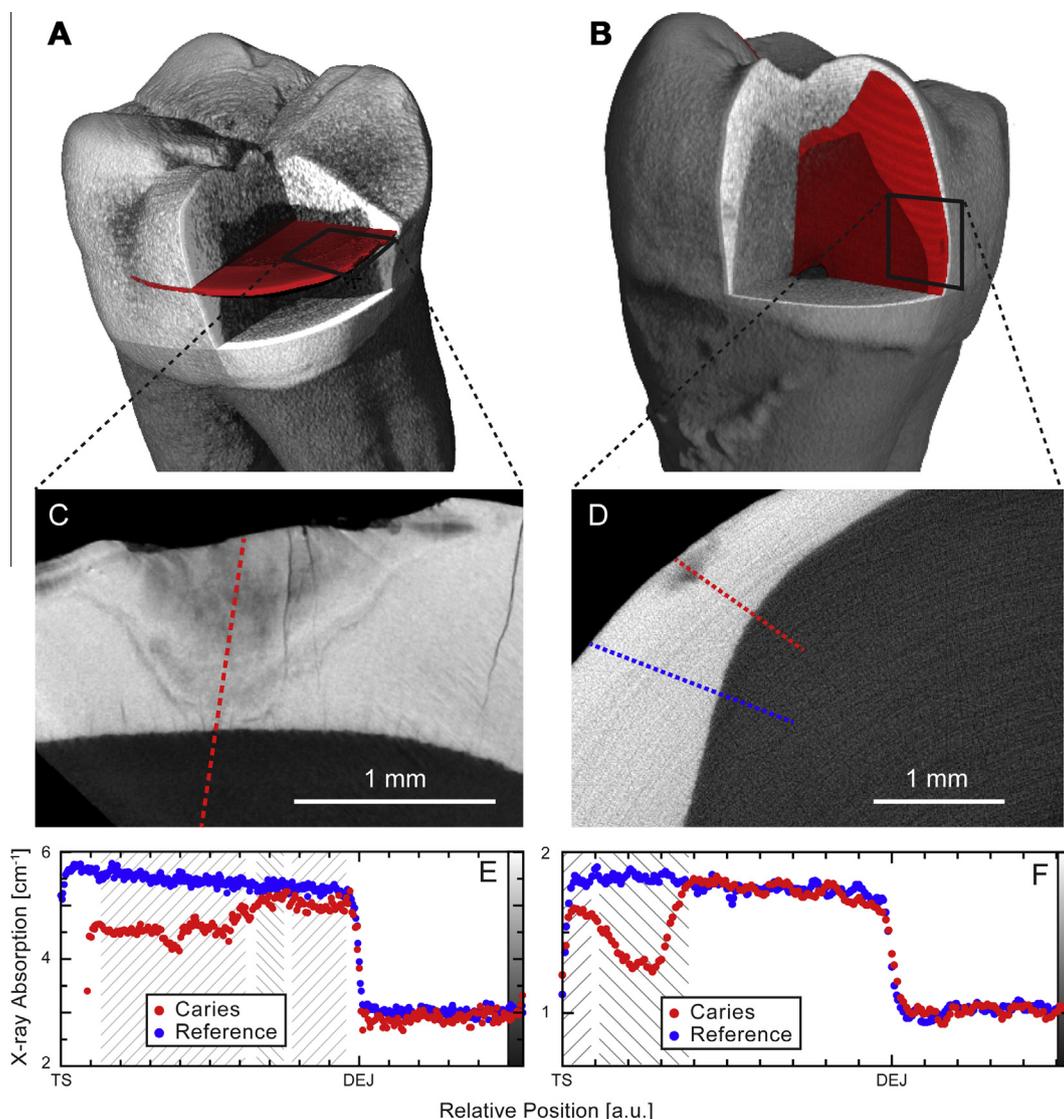
$$I(\phi) = I_0 + I_2 \cos(\phi + \Phi) \quad (1)$$

where  $I_0$  and  $I_2$  are the norm of the zero and second Fourier components, respectively, and  $\Phi$  is the phase of the second Fourier component. The data treatment is explained in detail elsewhere [39]. The data were treated using self-written MATLAB<sup>®</sup> (2011, The MathWorks, Natick, USA) routines.

The SAXS signal along radial lines through the carious lesions was plotted from  $0^\circ$  to  $45^\circ$  in the direction of maximum extension of the lesion in  $15^\circ$  increments. Control plots of sound tooth structure were made along radial lines of the same specimen, but because natural caries was studied, the control plots could not be made at the same site as the caries. Therefore, the control samples inevitably differed slightly from the carious samples with respect to enamel and dentin thickness and radius of curvature. Additionally, because the moderate caries specimen had lost some surface enamel, its outer endpoint, did not coincide with that of the intact controls. The following data fields were examined and plotted for sound control samples and for samples through the moderate and incipient carious lesions. The mean orientation of the scattering signal can be extracted from the phase term  $\Phi$  given in Eq. (3). The orientation of the scattering signal is generally perpendicular to the main orientation of the scattering structures, e.g., crystallites in dentin and enamel.

## 3. Results

The SAXS study includes results from two representative examples of the carious process: a moderate lesion with surface loss reaching dentin with a horizontal orientation (specimen H); and an early surface lesion with a vertical orientation (V). Both examples are smooth surface lesions. Control samples were taken from healthy unaffected enamel in the same tooth specimens.



**Fig. 1.** (A, B) Position of specimens H and V in a 3-D  $\mu$ CT rendering of the teeth. (C, D) Selected virtual cuts through the SR $\mu$ CT data of the tooth slices. The carious lesion in specimen H (C) can be identified as darker region in the enamel, extending from the TS to the dentin. The funnel-shaped subsurface lesion in specimen V (D) appears as darker spot near the outer limit of the enamel. (E, F) Line plots of X-ray absorption through the specimens according to the dashed lines in (B) and (C), respectively. The line through unaffected enamel in specimen H (C) lies outside the field of view. The abscissa was rescaled so that both the DEJ and TS were superimposed.

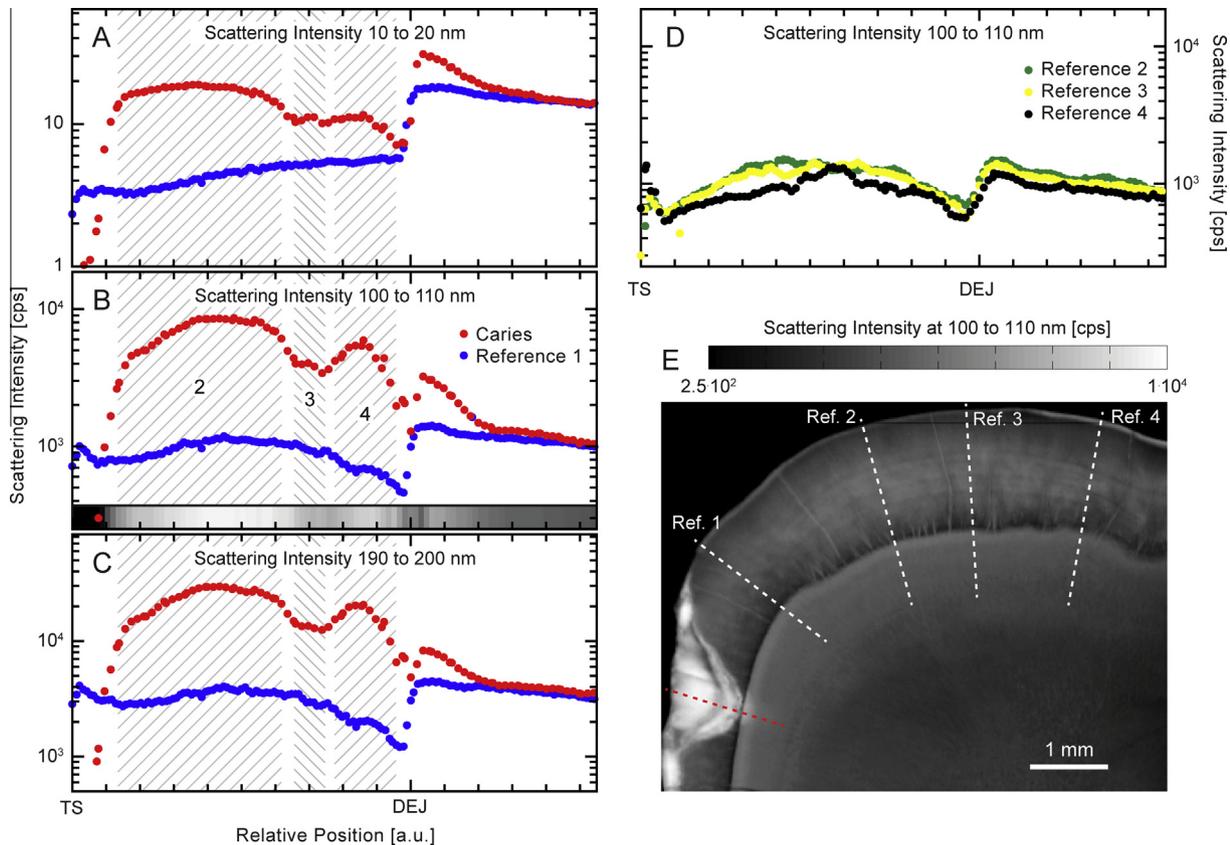
### 3.1. Moderate lesion reaching dentin, specimen H

Fig. 1 shows the position of specimens H and V within the corresponding teeth, in a three-dimensional (3-D)  $\mu$ CT rendering. Specimen H presented a moderate lesion extending to the dentin, as visible in the SR $\mu$ CT slice (Fig. 1C). The outermost surface enamel (zone 1) was intact at the peripheral borders of the lesion, but was absent from the central part of the lesion, probably as a result of the carious process. Within the remaining carious lesion, three additional zones were discerned; these were described by a profile of X-ray absorption through the center of the lesion (Fig. 1E). Zone 2 extended through half the thickness of the enamel and exhibited the lowest X-ray density, with a mean absorption corresponding to 86% of that of comparable unaffected enamel, and minima of 76%. Zone 3, a narrower band, deeper than and surrounding the first zone, showed X-ray absorption comparable with that of unaffected enamel, especially towards the sides of the lesion. Finally, zone 4, adjacent to the second and reaching the dentin, again displayed slightly decreased absorption with respect to unaffected enamel, with a mean of 93% and minima of 88%. Bands of alternating

X-ray absorption could be seen in the deeper parts of the lesions on both sides of its deepest extension.

The total scattered intensity is described in Fig. 2. Fig. 2A–C shows the intensity of the scattering signal on a line through the lesion (red dots) and one through unaffected enamel (blue dots), in the  $q$  ranges corresponding to 10–20 nm, 100–110 nm and 190–200 nm, respectively. The momentum transfer  $q$  is defined as  $q = \frac{4\pi}{\lambda} \sin(\theta)$ , where  $\lambda$  is the wavelength of the scattering X-rays, and  $\theta$  is the half scattering angle.  $q$  is related to the real space periodicity  $d$  by  $q = \frac{2\pi}{d}$ . Fig. 2D shows three profiles through unaffected enamel at different positions in the specimen (cf., image bottom right) in the range 100–110 nm. The abscissae of the plots were rescaled so that both the DEJ and tooth surface (TS) were superimposed. Little difference in scattered intensity plots could be discerned among the unaffected control samples.

Within the moderate carious lesion, distinct scattering intensity zones were discerned; they were largely coincident with the absorption zones, and are indicated by the shaded regions in Fig. 2A–C. Zone 2 exhibited high scattering in the body of the lesion, extending through half the enamel thickness; zone 3 was



**Fig. 2.** (A–C) Intensity of the scattering signal on a line through the lesion (red dots) and one through unaffected enamel (blue dots), in the ranges 10–20 nm, 100–110 nm and 190–200 nm, of specimen H, in counts per second according to the dashed lines in (E). Distinct scattering intensity zones can be discerned within the lesion, indicated by the shaded regions. (D) Three line plots through unaffected enamel at different positions in the specimen in the range 100–110 nm to demonstrate their similarity. (E) 2-D map of the total scattering intensity at scattering angles corresponding to the range 100–110 nm.

an intermediate band with reduced scattering; and zone 4 a region with increased scattering, approached the DEJ. Scattering intensities from zones 3 and 4 became more and more alike for smaller features in the 10–20 nm range. No such zones were found in unaffected healthy enamel over the ranges examined (Fig. 2A–D). The total scattered intensity of sound unaffected bulk enamel was almost an order of magnitude lower than the peak signal at the center of the body of the carious lesion. Table 1 summarizes the optical and X-ray scattering behavior of each zone.

As for all the plots in the present paper, additional data sets were created along lines rotated  $\pm 15^\circ$  from the central lines through the maximum extensions of the lesions depicted in Figs. 2 and 4–6 (data not shown). Little difference was found between these additional lines and the central lines; angled lines simply produced more oblique images of the same features.

In the narrow region of the DEJ interface, the plots of carious and unaffected control samples intersected (Fig. 2A–C). However, increased scattering intensity was found in the affected region of dentin immediately beneath the DEJ (Fig. 2A–C).

Scattered intensities for points belonging to the three carious zones ( $I_{car}$ ) and points from anatomically similar regions in healthy enamel ( $I_{sound}$ ) are compared in Fig. 3A. The ratio  $I_{car}/I_{sound}$  is plotted as a function of momentum transfer  $q$ . Zones 1 and 2 presented similar behavior, the ratio  $I_{car}/I_{sound}$  being constant over all but the smallest examined  $q$  ranges corresponding to periodicities  $< 50$  nm. For zone 2,  $I_{car}/I_{sound}$  amounted to about two-thirds of  $I_{car}/I_{sound}$  of zone 1. Zones 2 and 4 behaved in a like manner at periodicity ranges  $> 100$  nm. For smaller periodicities, the intensity in zone 4 decreased more rapidly than in zones 2 and 3.

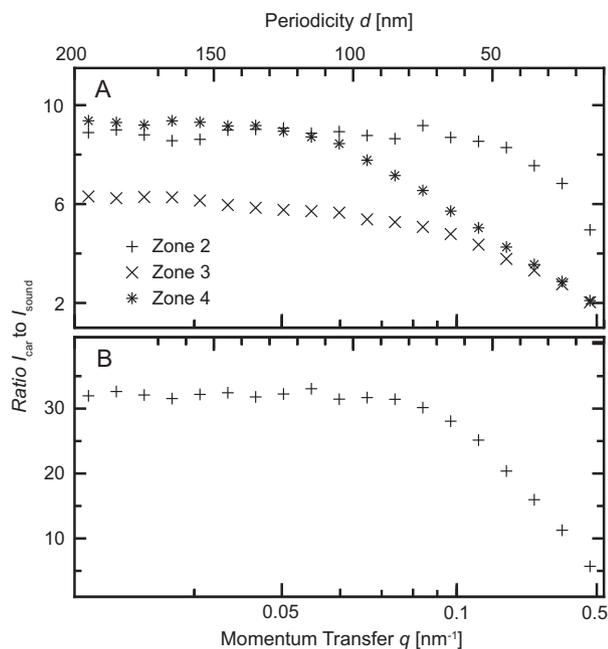
The mean orientation of scattering patterns [39] is displayed in Fig. 4. The color in the image (Fig. 4E) shows the orientation of the

**Table 1**  
Classification of carious zones comparing optical and X-ray scattering behavior.

	Pore size/distribution	Birefringence ([15,20,21])	X-ray absorption (with respect to unaffected enamel)	Scattering potential (with respect to unaffected enamel)
Zone 1	intact enamel <sup>a</sup>	Negative	Approximating unaffected enamel <sup>a</sup>	Approximating unaffected enamel <sup>a</sup>
Zone 2	Homogeneous pore size distribution between 50 and 200 nm	Positive	Reduced ( $\sim 75\%$ of unaffected enamel)	Over one order of magnitude higher
Zone 3	Homogeneous pore size distribution between 50 and 200 nm	Positive	Approximating unaffected enamel	About five times higher
Zone 4	Prevalence of larger pores (here above 100 nm)	Negative	Slightly reduced ( $\sim 93\%$ of unaffected enamel), with bands approximating unaffected enamel	Over one order of magnitude higher

<sup>a</sup> The statements concern specimen V.

main scattering signal for each point according to the color wheel. The line plots show the orientation of the scattering signal with respect to the dashed lines indicated in Fig. 4E, with  $0^\circ$  indicating a



**Fig. 3.** (A) Ratio  $I_{\text{car}}$  to  $I_{\text{sound}}$  of the scattering signal of a representative point in each carious zone  $I_{\text{car}}$  to a comparable point in healthy unaffected enamel  $I_{\text{sound}}$  as a function of the feature size  $d$  for specimen H. (B) Ratio  $I_{\text{car}}$  to  $I_{\text{sound}}$  for one point inside the lesion and a corresponding point in healthy unaffected enamel of specimen V as a function of momentum transfer  $q$ .

parallel alignment. Fig. 4A–C shows the orientation of the scattering signal in the ranges 10–20 nm, 100–110 nm and 190–200 nm, respectively, along a line through the lesion. A plot through unaffected healthy enamel, showing the orientation of the scattering signal related to features between 100 and 110 nm, is shown in Fig. 4D. The abscissae of the plots were rescaled so that both the DEJ and TS were superimposed. Carious enamel samples and their sound unaffected controls exhibited remarkably little difference in their values over the range of periodicities studied.

Fig. 5D shows the azimuthal plot around the direct beam of the total scattered intensity in a radial range corresponding to 100–110 nm, for a point in the caries (red dots) and in unaffected enamel (blue dots). The SAXS intensity is localized mainly along the equatorial direction of the crystallites (i.e., parallel to the TS) in both carious and unaffected enamel, giving rise to two distinct peaks. The increased intensity of the scattering signal from carious enamel is almost solely associated with the direction perpendicular to the crystallites, whereas the increase in intensity observed in all other directions was an order of magnitude smaller. The width of the peaks is related to the anisotropy of the scattering features within the specimen. For each raster scan point, the peaks were fitted with Gaussians and a constant background, and the FWHM was extracted. Fig. 5E shows the FWHM for each point in the range corresponding to 100–110 nm. In zone 2, slight changes to the FWHM of the equatorial scattering can be identified. The red and blue dots indicate the points from which the azimuthal intensity distribution in Fig. 5A was plotted. Fig. 5A–C shows the FWHM of the equatorial peaks in the ranges 10–20 nm, 100–110 nm and 190–200 nm, respectively, along a line through the lesion (red dots) and a line through unaffected enamel (blue dots). A slight decrease in the FWHM, i.e., an increase in SAXS anisotropy, can be found in the carious region, especially towards larger nanometer periodicities.

### 3.2. Early surface enamel lesion, specimen V

The orientation of the section of interest within the tooth is displayed in Fig. 1B. Selected slices through the SR $\mu$ CT data set of

specimen V are shown in Fig. 1D. The carious lesion was visible as a small darker region in the sub-surface enamel owing to reduced X-ray absorption. No surface loss was evident. Line plots showed that the absorption of the outermost surface of the lesion, zone 1, approximated that of unaffected controls; the body of the lesion, zone 2, exhibited a definite subsurface dip in X-ray absorption (Fig. 1F). In all other ways, X-ray absorption did not differ among control and lesion plots.

Total scattered intensity is described in Fig. 6A for the range 100–110 nm, along a line through the lesion (red dots) and through unaffected enamel (blue dots). Plots for the other examined ranges exhibited equivalent behavior (data not shown). The small early carious lesion differed from the moderate carious lesion. The very outermost surface enamel, zone 1, indicated by the shaded region labeled 1, approximated the control samples, and a single narrow sharp spike in scattered intensity, the body of the lesion, was localized to the outer half of the enamel thickness, indicated by the shaded region labeled 2.

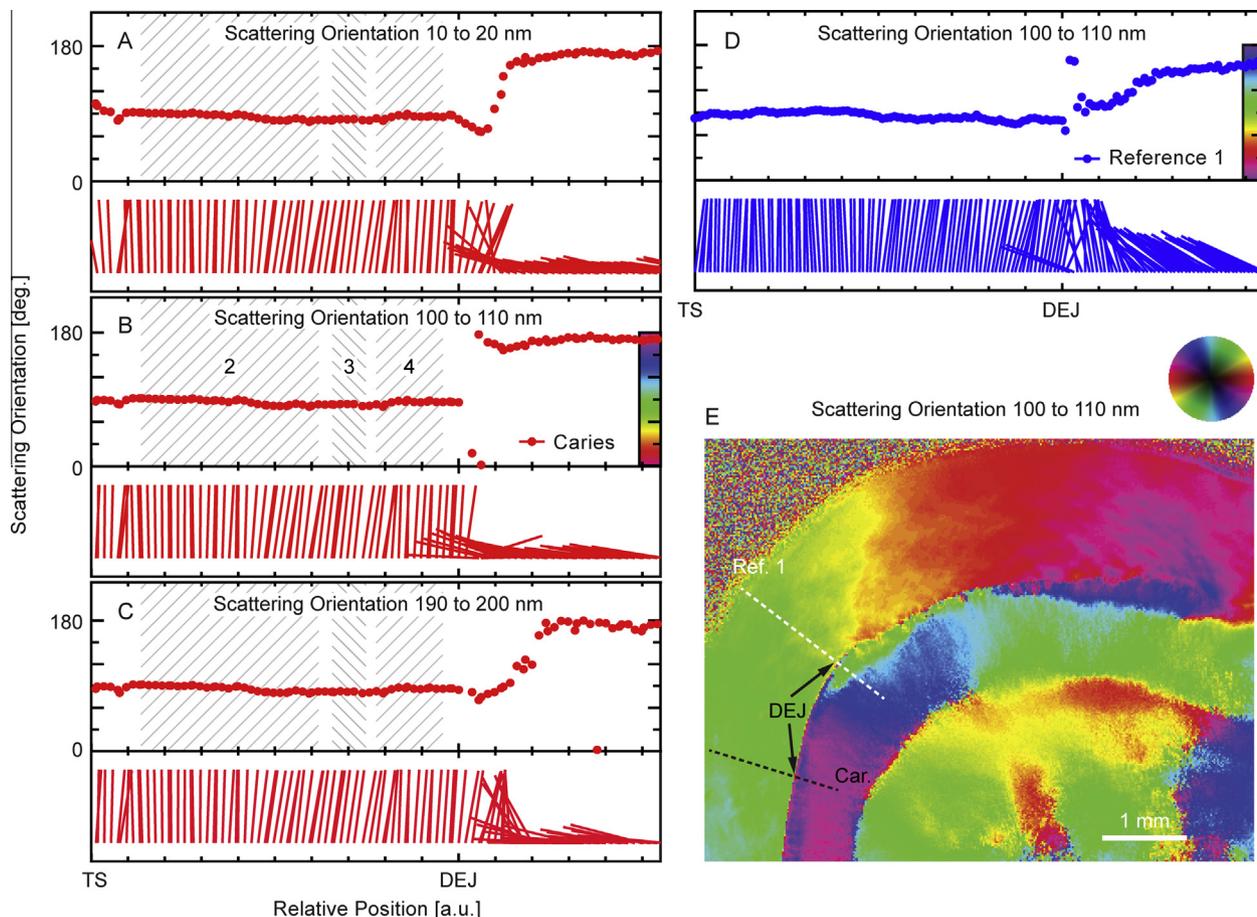
Fig. 3B, shows the ratio  $I_{\text{car}}/I_{\text{sound}}$  for a point inside the small lesion and a comparable point in healthy enamel, analogously to the three regions of the moderate lesion. The ratio keeps a constant value for periodicities down to 100 nm, and decreases towards larger scattering angles, analogous behavior to zone 2 in the moderate lesion.

The angle of scattering signals in the range 100–110 nm with respect to a radial line is displayed in Fig. 6C (through the carious lesion) and D (through healthy unaffected tissue). Little difference could be discerned between values from the carious region and their controls. These data are shown in separate plots for the sake of clarity. Plots for the other examined ranges exhibited equivalent behavior (data not shown). Anisotropy, as extracted from the FWHM of the equatorial scattering (cf., Fig. 5), is shown in Fig. 6B, along a line through the lesion (red dots), and one through unaffected enamel (blue dots). The FWHM for each raster scan point in the range 100–110 nm is shown in Fig. 6F. The carious lesion is visible as slightly darker zone near the TS.

## 4. Discussion

### 4.1. Zone classification

Absorption data were consistent with prior radiographic analyses. The small early lesion had a narrow dip in absorption that was sharply localized to a zone just beneath the relatively normal outermost enamel. These results suggest that, in these real-life carious lesions, the outermost enamel can readily re-mineralize, or even hyper-mineralize in an appropriate environment [7]. Many prior studies profiling carious lesions have shown increased X-ray density, increased mineralization, micro- and nano-hardness of zone 1 surface enamel [9,10,12–14,16,41–43]. Physicochemical phenomena and protection by saliva seem the most likely reasons for the fortification of the outermost enamel [7,44]. Although surface protection does not occur in all cases, it has been reported in both naturally occurring and artificial lesions [9,10,12–14,16,41–44]. However, re- or hyper-mineralization of the outermost enamel is a double-edged sword: it prevents substrates, calcium and phosphate ions, reaching the deeper parts of the lesion, thus preventing re-mineralization of deeper parts of the lesion. The moderate lesion demonstrated the additional complexity of the bulk and deepest parts of the enamel lesion being separated by an intermediate denser and thus less porous zone and containing several alternating layers or laminations, displayed as layers of alternating X-ray density (Fig. 1) [45]. The laminations may have been produced by successive periods of cyclic de- and re-mineralization over differing time periods when the environment may have favored one or other process [45].



**Fig. 4.** (A–C) Orientation of the scattering signal along the black dashed line indicated in the image (E). The values given correspond to the angle between the main orientation of the scattering signal and the black dashed radial line, with  $0^\circ$  indicating a parallel alignment. Plots (A–C) show the orientation of the scattering signal in the ranges 10–20 nm, 100–110 nm and 190–200 nm, respectively. The vector plots demonstrate the perpendicular alignment of the scattering signal to the radial line in enamel. The shaded regions correspond to the zones as identified in Fig. 2. (D) Orientation of the scattering signal along a line through unaffected healthy enamel, in the range 100–110 nm, cf., white dashed line in (E). (E) 2-D map of the orientation of the scattering signal at scattering angles corresponding to the range 100–110 nm, according to the color wheel.

Differences in birefringence due to the production of submicroscopic pores during de-mineralization have been used to segment the smooth surface carious enamel lesion into four zones: the outer surface (zone 1), the body of the lesion (zone 2), the dark zone (zone 3), and the translucent zone (zone 4) [15,20,21]. Most of the outermost enamel surface of the moderate lesion, zone 1, had been lost and thus was not studied. However, the remaining lesion was divisible by absorption and scattering intensity into zones broadly coincident with those defined by differences in optical birefringence [15,20,21]. In the small early lesion, zones 1 and 2 were evident and broadly coincident with those defined by differences in optical birefringence.

Since both methods are sensitive to the presence of pores within the calcium phosphate phases of the enamel, the assumption that the zones coincide is reasonable. As optical birefringence, related to the wavelength of visible light, it is relatively sensitive to long-range orders in comparison with SAXS, the methods are complementary.

#### 4.2. Pore size distribution

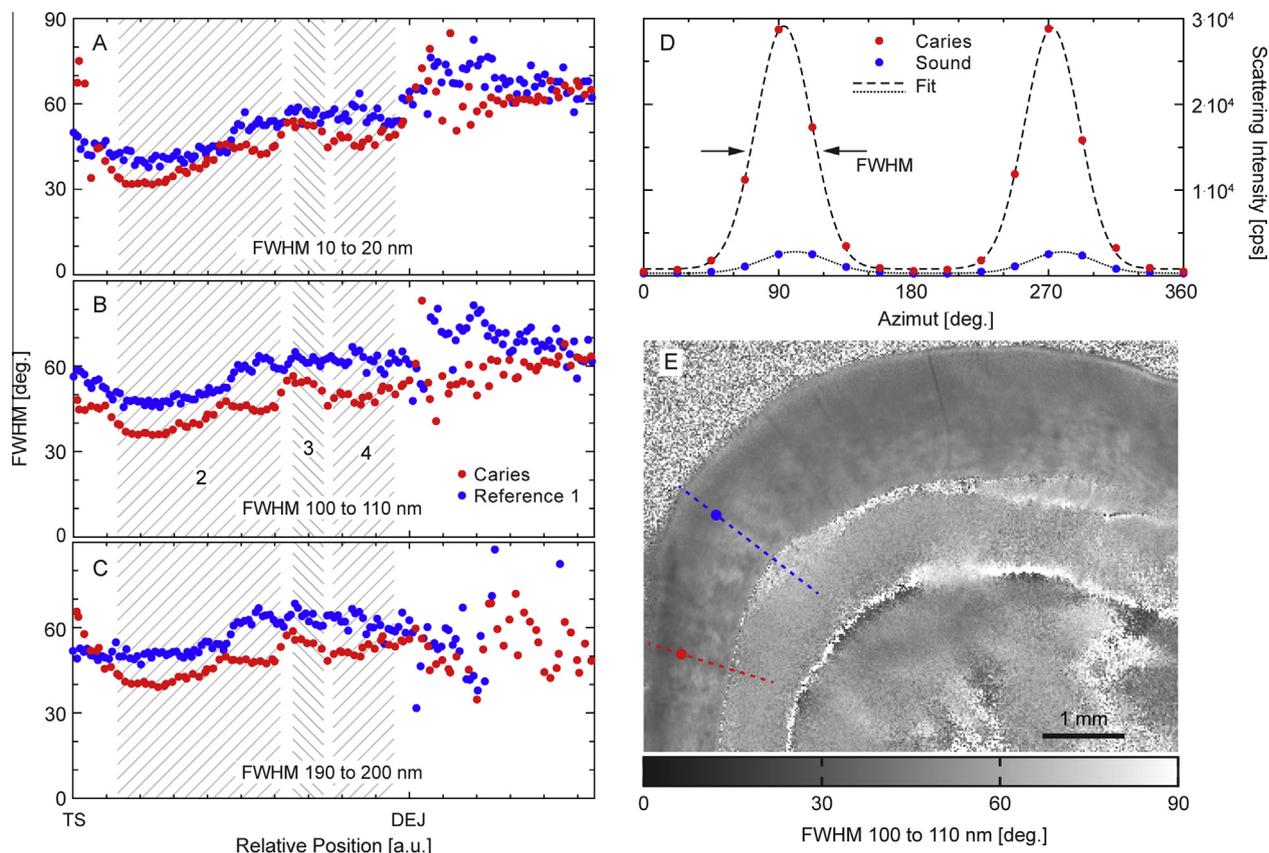
The increase in the abundance of pores in carious tooth structures must be considered to be a primary defining feature of the carious process. Accordingly, an increased scattered intensity in carious dentin [31] and enamel [35] has been reported. Since the

SAXS signal intensity is not homogeneous across the thickness of the enamel, the ratio  $I_{\text{car}}/I_{\text{sound}}$  of the SAXS signal from the carious lesion and from an anatomically equivalent region was chosen to illustrate changes in scattering behavior.

In zone 4 of the moderate lesion, generally consistent with the translucent zone,  $I_{\text{car}}/I_{\text{sound}}$  decreased markedly  $<100$  nm, indicative of larger pores. The fact that the  $I_{\text{car}}/I_{\text{sound}}$  was constant for all investigated nanometer ranges except the smallest ones  $<50$  nm in both zones 2 and 3 suggests the presence of a more homogeneous distribution of pore sizes in the investigated range 200–50 nm.

It has been hypothesized that, in the outer regions of surface caries and, notably, in the dark zone (zone 3), some degree of re-mineralization occurs [46], or that the redistribution of endogenous organic material inside the lesion leads to increased mineral content [47]. This similar behavior of the ratio  $I_{\text{car}}/I_{\text{sound}}$  as a function of scattering angle in zones 2 and 3 is indicative of a similar caries-induced destruction pattern, consisting of larger and smaller pores, where the smaller ones are the result of partially re-mineralized larger voids [45,48]. The higher scattered intensity in zone 1 arises from a more advanced status of enamel deterioration, i.e., a higher density of pores, in agreement with its reduced X-ray density. The decreased number of pores in zone 2 is partly due to natural re-mineralization.

The findings represented in Figs. 1–6 are consistent with the traditional models of the carious lesion derived from light microscopy,



**Fig. 5.** (A–C) FWHM value of the azimuthal SAXS intensity distribution in the ranges 10–20 nm, 100–110 nm and 190–200 nm, respectively, along a line through the lesion (red dots) and one through unaffected enamel (blue dots, cf., (E)). The FWHM value determination is illustrated in (D). (D) SAXS intensity as function of the azimuthal angle around the central beam, for a point in the lesion (red-colored dots) and one in healthy enamel (blue-colored dots) of specimen H, according to (E). The intensity distribution was fitted with two Gaussians and a background. (E) The FWHM of the Gaussians was extracted for each raster scan point. Zone 1 of the lesion appears slightly darker than unaffected enamel, indicating increased anisotropy of the scattering signal.

microradiography and microhardness profiles [12], but have advanced knowledge in defining the underlying nanostructures.

Despite increased porosity and decreased density in the enamel and dentin immediately adjacent to the DEJ, the scattering intensity and absorption plots for carious and unaffected control samples intersected at this internal interface. The DEJ, a most remarkable structure, durably unites extremely dissimilar biomaterials, enamel and dentin, preventing crack propagation from brittle enamel into dentin, and preventing interfacial delamination [49–52]. This finding has extremely important implications for the restorative strategies used to address carious teeth, suggesting that ultraconservative approaches, beyond current minimally invasive approaches [53], could preserve an intact DEJ, even if bounded on both sides by partly de-mineralized tissues.

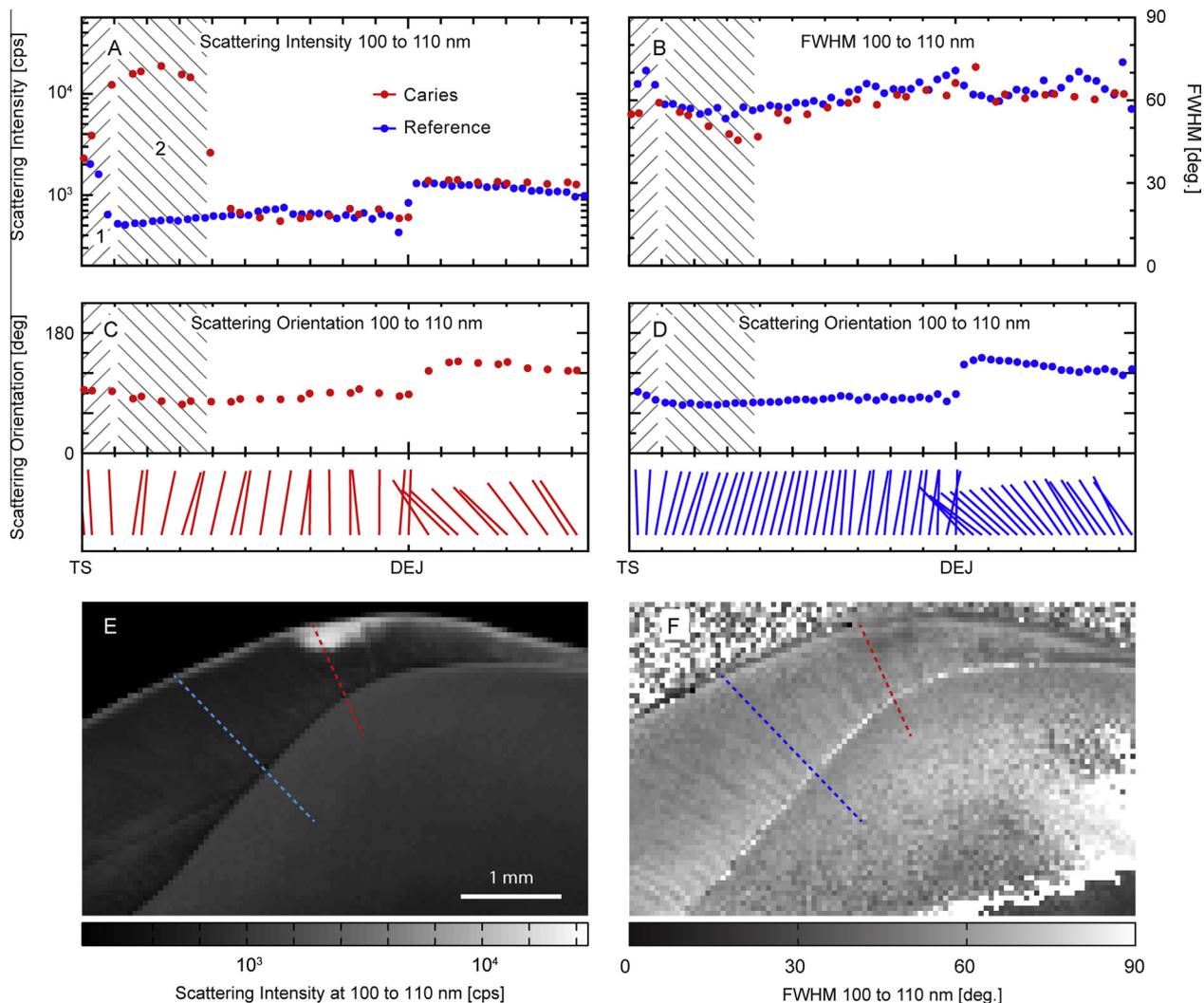
In the small early lesion, only a slight decrease in X-ray density in the outermost enamel was observed; whereas, the body of the lesion had a marked decrease. The scattering signal intensity presented a similar but inverse behavior, being comparable with that from healthy enamel at the surface of the tooth and increasing with decreasing X-ray density of the specimen. The  $I_{\text{car}}/I_{\text{sound}}$  behavior is similar to that found in the fourth, deepest zone in the moderate lesion. The ratio  $I_{\text{car}}/I_{\text{sound}}$  is higher for small scattering angles, i.e., periodicities >100 nm. This similarity indicates that both the subsurface body lesion and the deepest zone in the moderate lesion are cases of early caries attack, and a similar pore size distribution can be expected.

#### 4.3. Nanostructure orientation and anisotropy

The mean orientation of the scattering signal remained unchanged among carious and sound tooth structure in both early

and moderate carious lesions. The mean orientation of the scattering signal in healthy enamel was clearly related to the arrangement of the crystallites in the rods running from the DEJ towards TS, with their *c*-axis parallel to the crystallite long axis [54], the scattering signal being aligned perpendicularly to this direction. Apparently, the contribution of the interrod crystallites (rod sheaths and tails) is less than the scattering from the highly ordered and closely packed crystallites within the rod body [55–60].

As illustrated in Fig. 5, caries-induced changes only slightly modify the SAXS signal anisotropy, towards higher anisotropy. The distinction was more marked in zone 2, where the highest degree of de-mineralization was found. Similarly, in the subsurface lesion in specimen V, where the de-mineralization reached 25%, a slight increase in anisotropy was observed. Here, the selective hollowing [61] and complete dissolution of individual crystallites within the rods leads to the increased equatorial scattering, parallel to the DEJ, while increase in scattering signal from the more resistant interrod crystallites is less prominent. In zone 3, where a certain degree of re-mineralization has taken place, the FWHM of the SAXS approximates that of unaffected enamel, i.e., anisotropy is decreased compared with zone 2, indicating that re-deposition processes give rise to at least partially isotropic structures. While the convergence between the FWHM values in carious and healthy tissues might indicate the restoration of tooth morphology through the naturally occurring re-mineralization, this does not necessarily mean that this is actually the case, since it is impossible to determine from the SAXS signal whether the re-deposition of material is happening preferentially at certain locations, such as within the rod or the interrod. The SAXS signal appears highly anisotropic, however, indicating that despite de- and re-minerali-



**Fig. 6.** Combined plots for specimen V. (A) Intensity of the scattering signal on a line through the lesion (red dots) and one through unaffected enamel (blue dots), in the range 100–110 nm, according to (E). The scattering signal in the outermost carious enamel, indicated by the shaded region labeled 1, approximates that of healthy enamel. The body of the carious lesion, located in the outer half of the enamel and indicated by the shaded region labeled 2, yields an increased scattering signal. (B) FWHM of the azimuthal intensity distribution of the scattering signal on a line through the lesion (red dots) and one through healthy enamel (blue dots), in the range 100–110 nm according to (F). The inner 50% of the lesion exhibits increased anisotropy, i.e., a reduced FWHM value. (C, D) Orientation of the scattering signal along a line through the lesion (C) and one through healthy enamel (D), in the range 100–110 nm according to (E), with respect to the dotted lines in (E). The carious lesion cannot be readily distinguished. (E) 2-D map of the total scattered intensity in the range 100–110 nm for specimen V. The carious lesion appears as a bright spot at the enamel surface. (F) 2-D map of the FWHM of the azimuthal intensity distribution in the range 100–110 nm. The lesion exhibits slightly increased anisotropy compared with unaffected enamel.

zation processes in zone 3 much of the enamel nanostructure is retained. Zone 4 presents FWHM values close to those from unaffected enamel. Since only little re-mineralization can be expected in zone 4, it appears that, despite caries-induced destruction, the structural anisotropy of the affected enamel is preserved. The retention of organization, despite de-mineralization, has important implications for the potential for interventions to not only re-mineralize de-mineralized enamel, but to do so in the original organizational form at the nanostructural level.

#### 4.4. Confluence with classical caries models

Although the sample size was small, the lesions studied were carefully chosen to bracket the classically studied early carious lesion. The examination was performed in different perpendicular planes. The caries lesions were natural, probably occurring over years with innumerable cycles of de-mineralization and re-mineralization, rather than being artificially produced. They complemented prior SAXS data on fissure caries and an advanced

grossly cavitated lesion. Instead of a small amount of data on a large sample, this work produced an enormous amount of data (over 110,000 frames) on a small, but well-anchored, sample. It is important to note that the findings with respect to unaltered enamel were completely consistent with prior SAXS data on a variety of other teeth [33]; the data describing the studied lesions, early and moderate, in different planes, were entirely consistent with one-another and with classical models [9,10,12,14–16,20,21,31,35,41–43,45]. The findings were consistent with SAXS data previously reported for an advanced cavitated lesion and for fissure caries [33,36].

## 5. Conclusions

The fact that both orientation and anisotropy of the SAXS signal from carious enamel closely resembled those from unaffected regions reinforces the notion that naturally occurring de- and re-mineralization produce an anisotropic structure that retains the original nanoscale organization. This current SAXS data,

demonstrating the preservation of orientation in carious lesions, independent of degree of de-mineralization or pore morphology over 20–200 nm, advances understanding of the effects of de- and re-mineralization cycles at the crystallite level.

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### Appendix A. Figures with essential color discrimination

Certain figures in this article, particularly Fig. 2, are difficult to interpret in black and white. The full color images can be found in the on-line version, at <http://dx.doi.org/10.1016/j.actbio.2013.08.024>

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