## Viscoelastic properties of Polydimethylsiloxane studied by cantilever bending

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**INTRODUCTION:** The mechanical properties including viscoelasticity of micro- to nanometerthin polymer films are crucial for efficient, electrically activated polymer (EAP) actuators [1]. Here, we demonstrate the actuation response with the cantilever bending bar method [2] as a quantitative measure of the degree of cross-linking of Polydimethylsiloxane (PDMS) films. Siloxane-based polymers are well known for their elasticity with strains levels of up to 117 % and dielectric behavior [1]. Especially, the millisecond response [1] and biocompatibility make it suitable for biomimetic applications in the human body such as artificial muscles [3].

**METHODS:** The 4 µm-thin polymer films were spin-coated on Polyetheretherketone (PEEK) substrates (APTIV 2000, Victrex, Lancashire, UK) with a thickness of 25 µm embedded between sputtered electrodes. 15 nm-thin Au This asymmetric EAP-microstructure was characterized by applying a voltage [2]. The actuation mode is based on the COULOMB attraction between the oppositely charged electrodes. The squeeze of the incompressible polymer results in an expansion in x- and y-direction causing a torque of the cantilever, detected by a displacement of a reflected laser beam on a position sensitive detector. Cross-linking was realized through heat curing at curing temperatures of 80 °C.

**RESULTS:** The actuation of 0.5 h heat-cured Elastosil A/B over a period of 15 s is presented in Figure 1 for actuation voltages between 150 and 400 V. The deflection at 150 V applied voltage increases within a time period of 2 s before it reaches equilibrium. For higher actuation voltages of 300 V the maximal deflection increases according to the MAXWELL pressure quadratic with the applied voltage but drops down within a few seconds to equilibrium. The relaxation process can be characterized using the difference between maximal and equilibrated deflection d and the time constant  $\tau$ . The fitted exponential function  $d(t) = C \exp(-t/\tau)$  is included as a line into Figure 1. With a further increase to 400 V this effect becomes even more pronounced with a 43 % relaxation of the maximal deflection compared to a 23 % relaxation of deflection at 300 V. Furthermore this relaxation process slows down for higher applied strains to polymer network with

an increased time constant of  $\tau = (1.52 \pm 0.01)$  s at 400 V compared to  $\tau = (0.85 \pm 0.02)$  s at 300 V. For 2 h heat-cured polymer films no relaxation of the actuation under applied strain was observed.



*Fig. 1: Actuation of EAP-microstructures on PEEK cantilevers is presented for 0.5 h heat-cured polymer at actuation voltages of 150 to 400 V.* 

**DISCUSSION & CONCLUSIONS:** We found that polymeric thin films exhibit curing-timedependent compliance under strain. As completely cross-linked PDMS is known to be incompressible we relate this phenomenon to the degree of network cross-linking, which is increased with curing time. Thus, the presented cantilever bending method can deliver quantities about the viscoelastic properties of a polymer film.

REFERENCES: <sup>1</sup>R. Pelrine et al. (2000) Highspeed ellectrically actuaced elastomers with strain 100 %, greater than Science 287:836-839 <sup>2</sup>B. Osmani et al. (2015) Micro- and nanostructured electro-active polymer actuators as smart muscles for incontinence treatment, AIP Conf Proc **1646**:91-100 <sup>3</sup>B. Müller et al. (2009) The challenges in artificial muscle research to treat incontinence, Swiss Med Wkly 139:591-595 **ACKNOWLEDGEMENTS:** The financial support of the nano-tera.ch initiative *SmartSphincter* is gratefully acknowledged. Furthermore, the authors thank VICTREX for supporting us with PEEK films.

